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## WORK ENVIRONMENT IMPACT ON STRENGTH PRODUCTION FOR ACUTE LOW BACK PAIN SUBJECTS

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### Abstract

**Aim.** Acute low back pain (ALBP) is a major factor of disability among workers, causing absence from work and an increased medical care cost. The purpose of this study was to evaluate maximal isometric strength (MIS) differences between acute low back pain subjects with prolonged sitting jobs and demanding physical work jobs, for extension with pelvic stabilization (EPS) and flexion with pelvic stabilization (FPS).

**Methods.** Maximal isometric torque for EPS and FPS was measured at two positions (0 and 30-degree flexion angles) on 56 men. Subjects were assigned in four groups, two with ALBP, the first (n=14) with prolonged sitting jobs and the second (n=14) with demanding physical work jobs and the other two (controls) without ALBP, the first (n=14) with prolonged sitting jobs and the second (n=14) with demanding physical work jobs.

**Results.** ALBP subjects with prolonged sitting jobs and with demanding physical work jobs described lower MIS in both EPS and FPS, in both angles, relative to controls ( $p < 0.05$ ). ALBP subjects with prolonged sitting jobs had lower values of MIS in both EPS and FPS, in both angles, than ALBP subjects with demanding physical work jobs ( $p < 0.05$ ).

**Conclusions.** These data indicate that ALBP has impaired both ALBP groups in MIS production, than controls. Demanding physical work for ALBP subjects is a direct factor for greater MIS production, than ALBP subjects with prolonged sitting jobs, despite the presence of ALBP.

**Keywords:** pain, spine, flexion, extension, strength.

### Introduction

Anually the cost of medical care generated by back pain is increasing and it has been estimated to be a major health problem in today's society, being the leading cause of disability globally (Buchbinder R. et al., 2013).

The factors which may contribute to the risk of back pain are the lack of sleep, fatigue, emotional instability, substance abuse (alcohol (Samoladas, E., et al., 2018) and drugs), smoking (Al-Obaidi, S.M. et al., 2004; Gilgil, E., Kaçar, C., Bütün, B. et al., 2005), family problems, overweight, physical inactivity, physical activity performed incorrectly (excessive or incorrect movements), weak muscle endurance, continuous and very demanding physical activity at work, prolonged sitting, inaccurate chronic postures in orthostatic position, repeated backfall, flexion, twisting, pushing and/or lifting, prolonged driving vibrations (Bovenzi, M. and Zadini, A., 1992), increased chronic stress (chronic stress is releasing cortisol hormone, which is involved in muscle and tendon injury), low job satisfaction, low

motivation for work and mental fatigue (Bigos, S.J., Battie, M.C., Spengler, D.M. et al., 1992).

Back pain is the most frequent cause of limitation of physical activity (Wing, P.C., 2001) or physical demanding work in enclosed workshops (Volinn, E., 1997) among people with age less than 45 years old (McCoy, C.E. et al., 1997). The peak age for spine injuries, generated by weak trunk muscles, is 40 years old (Andersson, G.B.J. et al., 1995). Some authors show, that the incidence of low back pain has a peak age situated in the third decade of life, and the expansion increases until the age of 65 years (Golob, A. and Wipf, J., 2014).

Acute low back pain has an enormous impact in the quality of life (causing poor health), productivity and workers' absenteeism (number of work days lost), which can lead to a significant economic burden to the society and, respectively, to the individuals and their families (Lindgren L., 2003), not only in developed countries but also in developing countries (Galukande M. et al., 2006).

It seems that, the reasons in generating pain or avoiding physical activity, are a cognitive scheme that does not limit physical activity, but only requires the

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avoidance of some specific physical movements (Leonhardt C., Lehr D., Chenot J. F. et al., 2009). Pain and disability caused by pain are not only influenced by organic pathological problems but are also influenced by social and psychological factors (Vlaeyen J. W. S. and Crombez G., 1999). Fear of movement, injury or reinjury and associated avoidance behavior are closely related to the functional disability caused by acute pain and, also, to the pain intensity perception (Leeuw M., Houben R. M., Severeijns R. et al., 2007). Interventions aimed at reducing the pain-induced fear in the acute phase of low back problems can prevent and reduce the restrictions of activities participation and execution (including physical ones) and may have a positive effect in reducing the transition from the acute phase of pain to the chronic phase of pain recorded to the lumbar/thoracic spine (Swinkels-Meewisse I. E., Roelofs J., Schouten E. G. et al., 2006).

In US industry, occupational low back pain, with a number of occupational factors such as prolonged sitting and demanding physical work, both of them in combination with awkward postures, is still the primary problem (Murphy P.L. and Volinn E., 1999; Bobick T.G., 2000; Lis A.M., Black K.M., Korn H. et al., 2007). It has been suggested that sitting at work is a risk factor for low back pain, but with no difference then standing at work (Claus A., Hides J., Moseley G. L. et al., 2008; Makhsous M., Lin F., Bankard J. et al., 2009). The motifs that prolonged sitting at work could relate to low back pain are, uninterrupted low-intensity muscle contraction and the loss of muscle strength due to inactivity (Beach T.A., Parkinson R.J., Stothart J.P. et al., 2005). Demanding physical work jobs, like buildings or

shipyard construction, could lead to low back pain, especially for subjects who work with heavy loads or in narrow spaces (Watanabe S., Takahashi T., Takeba J. et al., 2018). The difference, in low back pain incidence, in low back pain intensity or in trunk strength, between subjects with prolonged sitting jobs and demanding physical work jobs is unclear. Therefore, the purpose of this study was to evaluate the differences in MIS production between ALBP subjects with prolonged sitting jobs and ALBP subjects with demanding physical work.

## Methods

### Subjects

This longitudinal study was conducted in Constanta. After the presentation of study aims and methods, fifty-six Romanian men, with no history of orthopedic or cardiovascular contraindications, assigned in four groups, volunteered for this investigation. The subjects with demanding physical work jobs were workers from buildings and shipyard construction and the subjects with prolonged sitting jobs were bank and accountant workers. Fourteen of these subjects (mean age  $36^{11} \pm 6^2$  (years months)) were assigned to ALBP with prolonged sitting jobs group and 14 subjects (mean age  $34^5 \pm 4^8$  (years months)) were assigned to ALBP with demanding physical work group; 14 subjects (mean age  $35^6 \pm 4^1$  (years months)) with prolonged sitting jobs, without ALBP and 14 subjects (mean age  $33^5 \pm 3^{12}$  (years months)) with demanding physical work, without ALBP, acted as controls. Characteristics of subjects by groups are shown in table 1. Written informed consent was obtained from all subjects.

**Table 1.** Characteristics of the subjects <sup>a</sup>

	<b>Prolonged sitting jobs ALBP (n=14)</b>	<b>Demanding physical work jobs ALBP (n=14)</b>	<b>Prolonged sitting jobs without ALBP (n=14)</b>	<b>Demanding physical work jobs without ALBP (n=14)</b>
Body height (m.)	1.76 ± 9.9	1.75 ± 7.9	1.73 ± 6.2	1.72 ± 8.6
Body weight (kg.)	86.8 ± 9.2	80.9 ± 8.5	81.8 ± 5.4	76.5 ± 8.5
BMI (kg/m <sup>2</sup> ) <sup>b</sup>	27.8 ± 1.5	26.2 ± 1.8	27.4 ± 2	25.6 ± 1.4
BF (%) <sup>c</sup>	26.7 ± 2.8	24.3 ± 4.1	27.2 ± 2.7	24.8 ± 2.3

<sup>a</sup> Values are means ± SD;

<sup>b</sup> body mass index;

<sup>c</sup> body fat.

### Testing

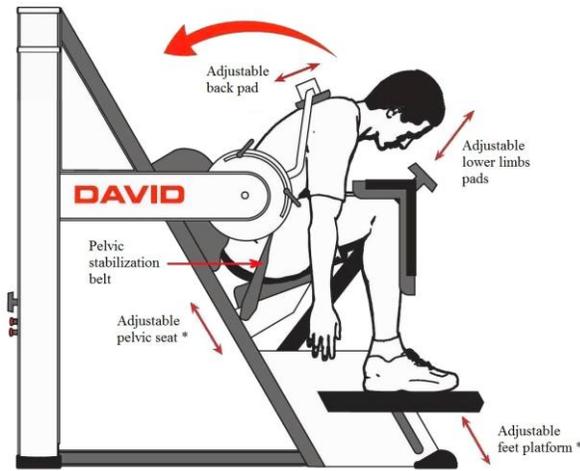
Each subject completed an MIS test on David F110 lumbar/thoracic EPS device (figure 1) and David F130 lumbar/thoracic FPS device (figure 2) (DAVID Fitness & Medical Ltd., Karitie 9, 01530 Vantaa, Finland). Each test included measurement of maximal voluntary isometric strength of trunk flexor and extensor muscles at

0° and 30° flexion angle. MIS values were recorded on MC-3 microcomputer (figure 3), which was connected to both David F110 lumbar/thoracic EPS and David F130 lumbar/thoracic FPS devices.

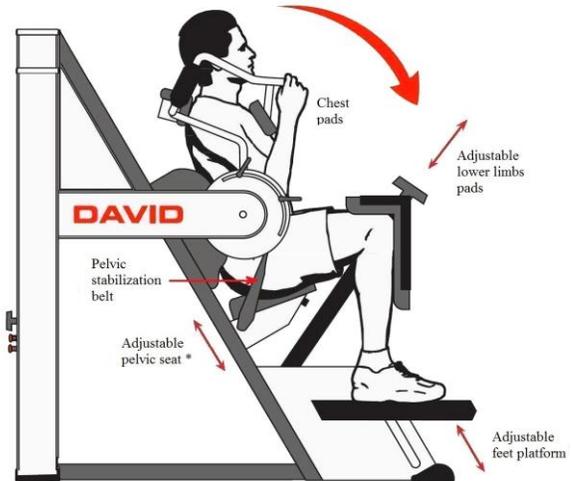
At this moment, the DAVID equipment, on which these MIS tests were performed, is one of the best. Reported to other companies (such as Panatta,

SportsArt), which produce such biomedical strength estimation devices, the David F110 lumbar/thoracic EPS and David F130 lumbar/thoracic FPS models have

received the highest scores in comparative assessment, from the point of view of ergonomics, comfort and movement biomechanics (Gottlob A., 2007).



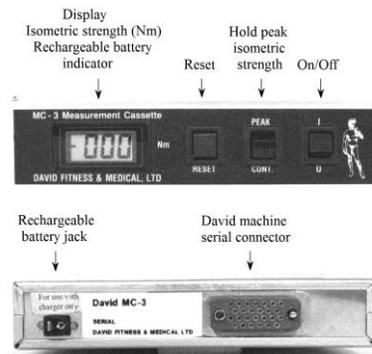
\* Feet and pelvic position is adjusted in rapport with subject height, to get an angle of approximately 90 degrees between thighs and calves.



\* Feet and pelvic position is adjusted in rapport with subject height, to get an angle of approximately 90 degrees between thighs and calves.

**Figure 1.** David F110 lumbar/thoracic EPS

**Figure 2.** David F110 lumbar/thoracic FPS



**Figure 3.** MC-3 digital test module

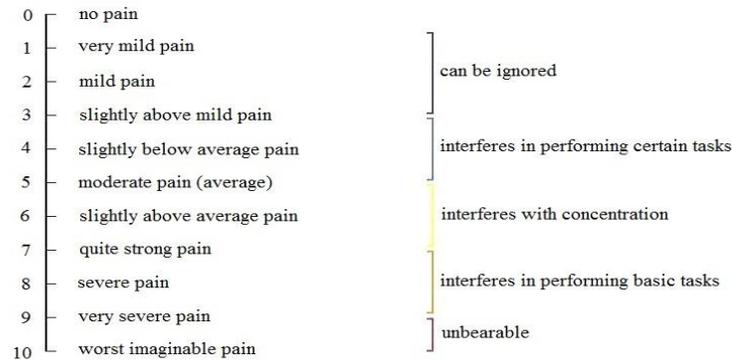
Subjects were seated in both David F110 lumbar/thoracic EPS and David F130 lumbar/thoracic FPS devices with their knees positioned so that the femurs were parallel to the seat, with the pelvis secured in place (stabilized) by a belt restraint. The lower limbs restraint consisted in an L shaped 90° pads on an adjustable crank, placed in the same time against the inferior and anterior side of the femurs and superior and anterior side of the tibia. These restraints were forcing the pelvis back against the seat. This restraining force stabilized the pelvis, allowing no lateral, vertical or rotational movement.

The subjects were instructed not to exercise for at least 24 hours before testing. To initiate the test on David F 110 lumbar/thoracic EPS device, subjects were first locked in 30° flexion angle and instructed to slowly and

continuously make extension of their back against the upper blades pad (movement arm of machine) for 2 to 3 second period, with arms beside the trunk. For David F 130 lumbar/thoracic FPS device, subjects were first locked in 0° angle and instructed to slowly and continuously make flexion of their trunk against the upper chest pads (movement arm of machine) for 2 to 3 second period, with hands firmly grasping the chest pads holders. Once maximal tension had been achieved, subjects were instructed to maintain the contraction for an additional 1 to 2 seconds before relaxing. A 5 to 10 minutes rest interval was provided until the next isometric contraction, while the next 0° and, respectively, 30° angles of measurement was set. During the contractions, subjects were verbally encouraged to give a maximum effort. Lower limbs restraint and pelvic

restraint were tightened if pelvic movement was

observed during testing, to ensure pelvic stabilization.



**Figure 4.** Subjective assessment pain scale

The subjective assessment of ALBP intensity was achieved immediately after performing the MIS tests on both devices and for both angles tested, only on subjects with ALBP. The subjects were instructed to point the place, in the subjective assessment pain scale, where they best describe the acute pain experienced during the MIS tests.

The subjective assessment of ALBP intensity was achieved using a combination of visual pain assessment scale, numerical scale (11 points) to estimate pain intensity and verbal pain assessment scale (figure 4). The visual pain assessment scale is a method of measuring acute or chronic pain. However, the visual pain assessment scale presents inconveniences, concretized by, the misunderstanding of the abstract concept of the 10cm line of visual estimation of pain, many of whom find it difficult to accurately estimate the correct distance between the two extremes of pain. Since the visual pain assessment scale has some practical limitations (Williamson A. and Hoggart B., 2005), we considered it necessary to use this visual pain assessment scale together with the numerical and verbal scale of pain intensity assessment, which describes (more accessible and understandable for the subjects) the intensity of pain in words, for each of the 11 points. Even though the verbal pain assessment scale is less sensitive than the visual pain estimation scale (Breivik E. K. et al. 2000), it seems that the visual pain assessment scale, verbal pain assessment scale (DeLoach L. J. et al., 1998; Soyannwo O. A. et al., 2000; Clark P. et al., 2003) and numerical scale to estimate pain intensity (Ponce de Leon S. et al., 2004) are strongly correlated with each other.

### Data analysis

Isometric strength was measured in units of torque (Nm). Means and standard deviations were calculated for MIS test results and subjective assessment of ALBP intensity scores. Between David F110 lumbar/thoracic EPS and David F130 lumbar/thoracic FPS devices in 0° and, respectively, 30° flexion angles, MIS results and, respectively, ALBP intensity scores comparisons were made using two-tailed dependent student t test. The same test was used for MIS results and, respectively, ALBP intensity scores comparisons, between 0° and 30° flexion angle, for each test device. Between groups, MIS results comparisons were made using one-way ANOVA for independent groups and post ANOVA Tukey HSD test for each test device and, respectively, test angle. Also, between groups, ALBP intensity scores comparisons were made using two-tailed independent student t test for each test device and, respectively, test angle. Statistical significance was accepted at  $p < 0.05$  (Lieber, R.L., 1990; Sheskin, D.J., 2004; Thomas, R.J. and Nelson, J.K., 1996).

### Results

Prolonged sitting jobs subjects with ALBP showed significantly lower values in MIS production ( $F(3, 52)=17.7$  for 0° test angle and  $F(3, 52)=17.9$  for 30° test angle) for trunk EPS, than all other groups. The same significantly lower values, for prolonged sitting jobs subjects with ALBP, were also reported for trunk FPS ( $F(3, 52)=11.8$  for 0° test angle and  $F(3, 52)=11.7$  for 30° test angle), than all other groups.

**Table 3.** Lumbar/thoracic extension and flexion MIS (Nm) values <sup>a</sup>

Subjects		Testing angles (deg)	David F110 Lumbar/thoracic EPS (Nm)	David F130 Lumbar/thoracic FPS (Nm)
ALBP	Prolonged sitting jobs (n=14)	0°	255.6 ± 25.9 <sup>b d f g</sup>	172.7 ± 22.3 <sup>c e</sup>
		30°	266.3 ± 23.8 <sup>b d g</sup>	185.2 ± 33 <sup>c e</sup>
	Demanding physical work (n=14)	0°	287.1 ± 17.6 <sup>d g</sup>	197.5 ± 20.1 <sup>e f</sup>
		30°	289.7 ± 24.7 <sup>d g</sup>	216.9 ± 25.5 <sup>e</sup>
Without ALBP	Prolonged sitting jobs (n=14)	0°	279.2 ± 18.1 <sup>b f g</sup>	196 ± 16.5 <sup>c f</sup>
		30°	290.7 ± 17.8 <sup>b g</sup>	213.2 ± 23.3 <sup>c</sup>
	Demanding physical work (n=14)	0°	313.5 ± 22 <sup>f g</sup>	221.3 ± 26.2 <sup>f</sup>
		30°	326.2 ± 20.3 <sup>g</sup>	243.5 ± 20.7

<sup>a</sup> Values are means ± SD.

<sup>b</sup> compared with demanding physical work subjects, for 0° and, respectively, 30° testing angles, p<0.05;

<sup>c</sup> compared with demanding physical work subjects, for 0° and, respectively, 30° testing angles, p<0.05;

<sup>d</sup> compared with subjects without ALBP, for prolonged sitting jobs and, respectively, demanding physical jobs, for each corresponding testing angle, p<0.05;

<sup>e</sup> compared with subjects without ALBP, for prolonged sitting jobs and, respectively, demanding physical jobs, for each corresponding testing angle, p<0.05;

<sup>f</sup> compared with 30° testing angle, p<0.05;

<sup>g</sup> compared with David F130 Lumbar/thoracic FPS, p<0.05.

Values in MIS production, for trunk EPS, were significantly higher for all subjects and all testing angles, than trunk FPS MIS values (prolonged sitting jobs subjects with ALBP, t=22.4 for 0° test angle and t=8.8 for 30° test angle; demanding physical work subjects with ALBP, t=56 for 0° test angle and t=6.3 for 30° test angle; prolonged sitting jobs subjects without ALBP, t=22.1 for 0° test angle and t=40.6 for 30° test angle; demanding physical work subjects with ALBP, t=33 for 0° test angle and t=49.4 for 30° test angle). MIS results, for trunk FPS and, respectively, trunk EPS, were significantly higher for 30° test angle, than 0° test angle,

for all subjects without ALBP (prolonged sitting jobs subjects t=7.5 and demanding physical work subjects t=7.5 for David F110 lumbar/thoracic EPS; prolonged sitting jobs subjects t=4.2 and demanding physical work subjects t=5.5 for David F130 lumbar/thoracic FPS). In contrast, only prolonged sitting jobs subjects with ALBP had significantly higher MIS results for 30° test angle, than 0° test angle in trunk EPS (t=5.3) and, only, demanding physical work subjects with ALBP had significantly higher MIS results for 30° test angle, than 0° test angle in trunk FPS (t=2.9).

**Table 4.** Subjective ALBP assessment results <sup>a</sup>

Subjects		Testing angles (deg) <sup>f</sup>	David F110 Lumbar/thoracic EPS	David F130 Lumbar/thoracic FPS
ALBP	Prolonged sitting jobs (n=14)	0°	6.3 ± 1.1 <sup>c d</sup>	5.5 ± 1.1 <sup>b d</sup>
		30°	6.3 ± 1 <sup>c d</sup>	5.8 ± 1.2 <sup>d</sup>
	Demanding physical work (n=14)	0°	5.3 ± 0.9 <sup>c</sup>	4 ± 0.7 <sup>b</sup>
		30°	5.4 ± 0.8 <sup>c</sup>	4.3 ± 0.6

<sup>a</sup> Values are means ± SD.

<sup>b</sup> compared with 30° testing angle, for demanding physical work subjects and, respectively, prolonged sitting jobs subjects, p<0.05;

<sup>c</sup> compared with David F130 lumbar/thoracic FPS, for prolonged sitting jobs and, respectively, demanding physical work subjects, for each corresponding testing angle, p<0.05;

<sup>d</sup> compared with demanding physical work subjects, for David F110 lumbar/thoracic EPS and, respectively, David F130 lumbar/thoracic FPS, for each corresponding testing angle, p<0.05.

All ALBP subjects showed significantly higher values of subjective assessment of ALBP intensity for David F110 lumbar/thoracic EPS, than David F130 lumbar/thoracic FPS, in both angles tested (prolonged sitting jobs subjects,  $t=4.4$  for  $0^\circ$  test angle and  $t=3.5$  for  $30^\circ$  test angle; demanding physical work subjects,  $t=6.7$  for  $0^\circ$  test angle and  $t=7.8$  for  $30^\circ$  test angle). Also, prolonged sitting jobs subjects with ALBP showed significantly higher values of subjective assessment of ALBP intensity than demanding physical work subjects with ALBP, on both testing devices and, respectively, both angles tested (David F110 lumbar/thoracic EPS,  $t=2.4$  for  $0^\circ$  test angle and  $t=2.7$  for  $30^\circ$  test angle; David F130 lumbar/thoracic FPS,  $t=4.1$  for  $0^\circ$  test angle and  $t=4$  for  $30^\circ$  test angle).

All ALBP subjects showed significantly higher values of subjective assessment of ALBP intensity for  $30^\circ$  testing angle, than  $0^\circ$  testing angle, but only for David F130 lumbar/thoracic FPS (prolonged sitting jobs subjects,  $t=2.2$  and demanding physical work subjects,  $t=2.8$ ).

### Discussion

Prolonged sitting jobs subjects showed lower values of MIS production, than demanding physical work subjects on both EPS and FPS, despite the presence or not of ALBP. A demanding physical work produces a more pronounced flexion and extension trunk muscles strength development, compared to the sedentary work.

Both ALBP prolonged sitting jobs and demanding physical work subjects showed lower values of MIS production, than controls. It seems that, in chronic and acute low back pain subjects, lumbar extensor muscle strength control is compromised (Pranata A. et al., 2017). Some researchers showed that weak muscle strength is not generated by muscle incapability to produce muscle strength, but, rather, by the problems encountered in motor control (Jull G. A. and Richardson C. A., 2000), especially in low back pain subjects (Hodges P. W. and Richardson C. A., 1996). Nissan M, Bar-Ilan K., Brown S. et al., (2000), have shown that the generation of MIS is different between the subjects with low back pain and healthy subjects. Subjects with age over 40 years, with chronic low back pain, has a lower muscle strength for trunk flexion and extension (more marked for extension movement), compared with controls (subjects without low back pain) (Handa N. et al., 2000).

Trunk EPS muscles produced higher values of MIS, than trunk FPS muscles, for all subjects. Keller T. S. and Roy A. L. (2002), Straton A., (2007, 2009), Straton A. and Cismaş G., (2009), Hasue M., Fujiwara M., Kikuchi S. (1980) and Smidt G. L., Amundsen L. R., Dostal W. F. (1980), confirms that trunk extension muscles generate a significantly higher strength production, than the trunk flexion muscles.

All subjects showed lower values of MIS production in  $0^\circ$  testing angle, than  $30^\circ$  testing angle, on both FPS and EPS. Keller T. S. and Roy A. L., (2002) showed that for the flexion movement the MIS values are recorded at angles between  $20^\circ$  and  $30^\circ$  and for the extension movement the MIS values are recorded at an angle of  $50^\circ$ . The most effective angle of extension muscle strength development is  $36^\circ$  (Graves J. E., Pollock M. L., Leggett S. H. et al., 1992). Straton A. and Cismaş G., in a study conducted on the same DAVID devices, showed that, the highest values of MIS production were made at the  $30^\circ$  angle for flexion and extension movements. In contrast, Wessel J., Ford D., van Driesum D., (1994), concluded that, the production of isometric force, for flexion movement, decreases with the increase of the trunk flexion angle. However, there are still many controversies regarding the optimal angle setting in which the MIS highest value is estimated, due to the many positions of the body (and, implicitly, the body segments), as well as the stabilization possibility, or not, of the various joint rotational axis, when performing the MIS estimation tests.

All ALBP subjects perceived higher values in subjective ALBP assessment for EPS, than FPS. Kakaanpää M., Taimela S., Laaksonen D., et al., (1998), showed that subjects with chronic low back pain perceive higher pain intensity, when performing the MIS test for trunk extension movement at  $30^\circ$  test angle. In contrast, Renkawitz T., Boluki D., Grifka J., (2006) found that, the estimation of MIS for trunk extension movement, in athletes, has no relation to the presence of low back pain or to the neuromuscular disbalance of the right and left spine extension muscles.

Prolonged sitting jobs subjects with ALBP perceived higher values in subjective ALBP assessment, than demanding physical work subjects with ALBP, on both EPS and FPS. It seems that, demanding physical work subjects have a higher threshold of pain tolerance, than prolonged sitting jobs subjects, probably due to the harsh environment in which the subjects work.

### Conclusion

ALBP subjects with prolonged sitting jobs have lower values in MIS production and higher values of subjective assessment of ALBP intensity, than ALBP subjects with demanding physical work, in both EPS and FPS. ALBP is not a factor that influences the difference in MIS production between subjects with prolonged sitting jobs and subjects with demanding physical work.

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